

### Background

ACL injury is a common knee injury. The ACL is a ligament that connects the femur to the tibia. It is responsible for preventing the tibia from moving too far forward. ACL injury can lead to instability and pain. This study aims to compare the strain distribution in native ACL and reconstructed ACL in response to external knee loading.

### Methods

16 fresh-frozen cadaveric knee joints (70.3 ± 10.5 years) were used. 10 knees were intact and 6 were reconstructed. The ACL was instrumented with 20 strain gauges. The knee was loaded with 100 N of anterior tibial load and 5 Nm/10 Nm of internal/valgus torque. Strain was measured at full extension and 30 degrees of flexion.

### Materials & Methods

- Subjects: 16 fresh-frozen cadaveric knee joints (70.3 ± 10.5 years) (Intact: 10 knees, Reconstructed: 6 knees)
- 1. Biomechanical tests
  - 6-DOF robotic testing system
    - Loading conditions
      - 100 N of anterior tibial load
      - 5 Nm/10 Nm of internal/valgus torque (simulated pivot shift)
    - Measured strain in native ACL or reconstructed ACL at full extension and 30 degrees of flexion

### 2. Strain measurement

- Rotational stereoscopic image method (Figure 1, [3])
  - Fiber strains measured in 20 regions (Figure 2)

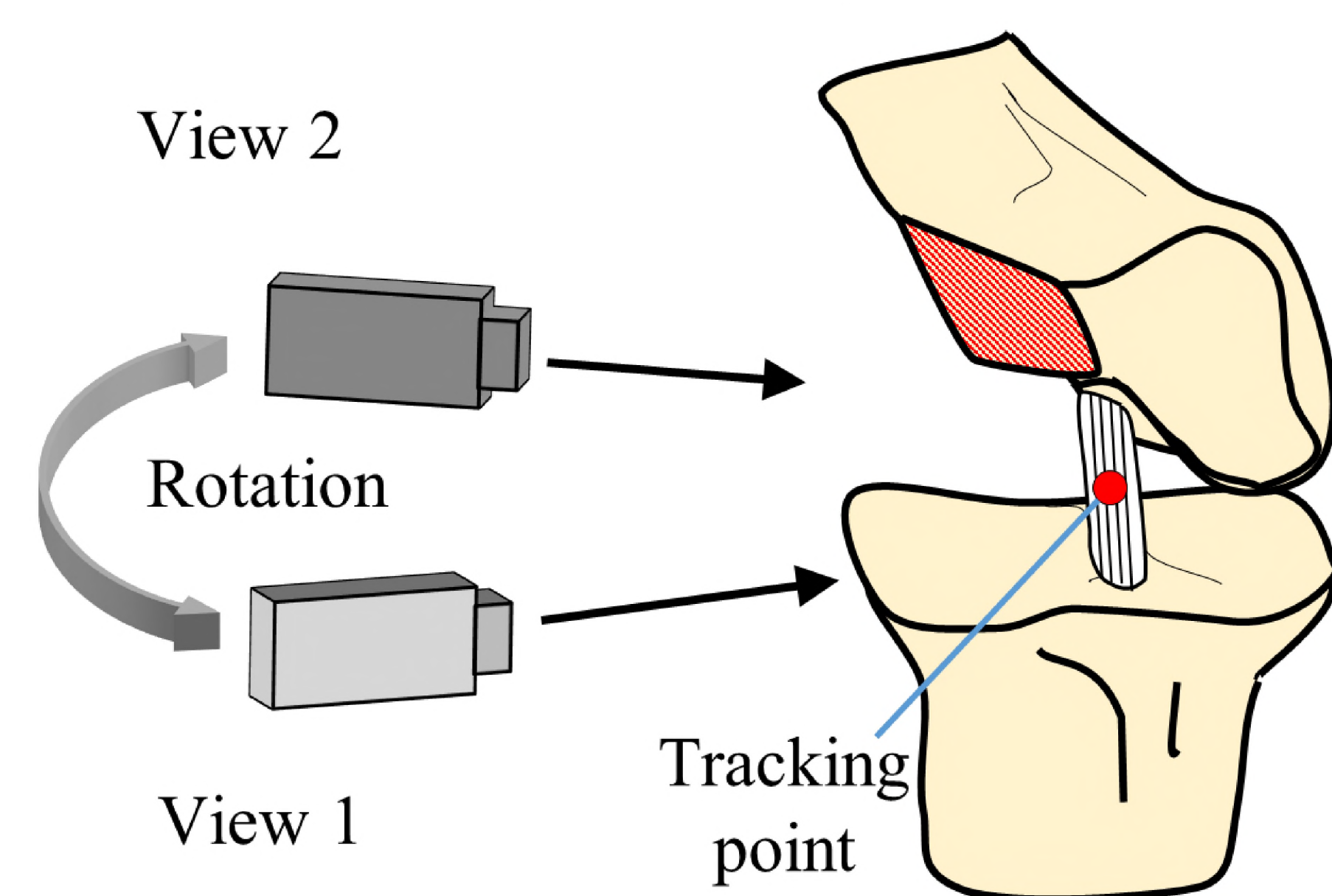


Figure 1: Schematic drawing of the rotational stereoscopic image method

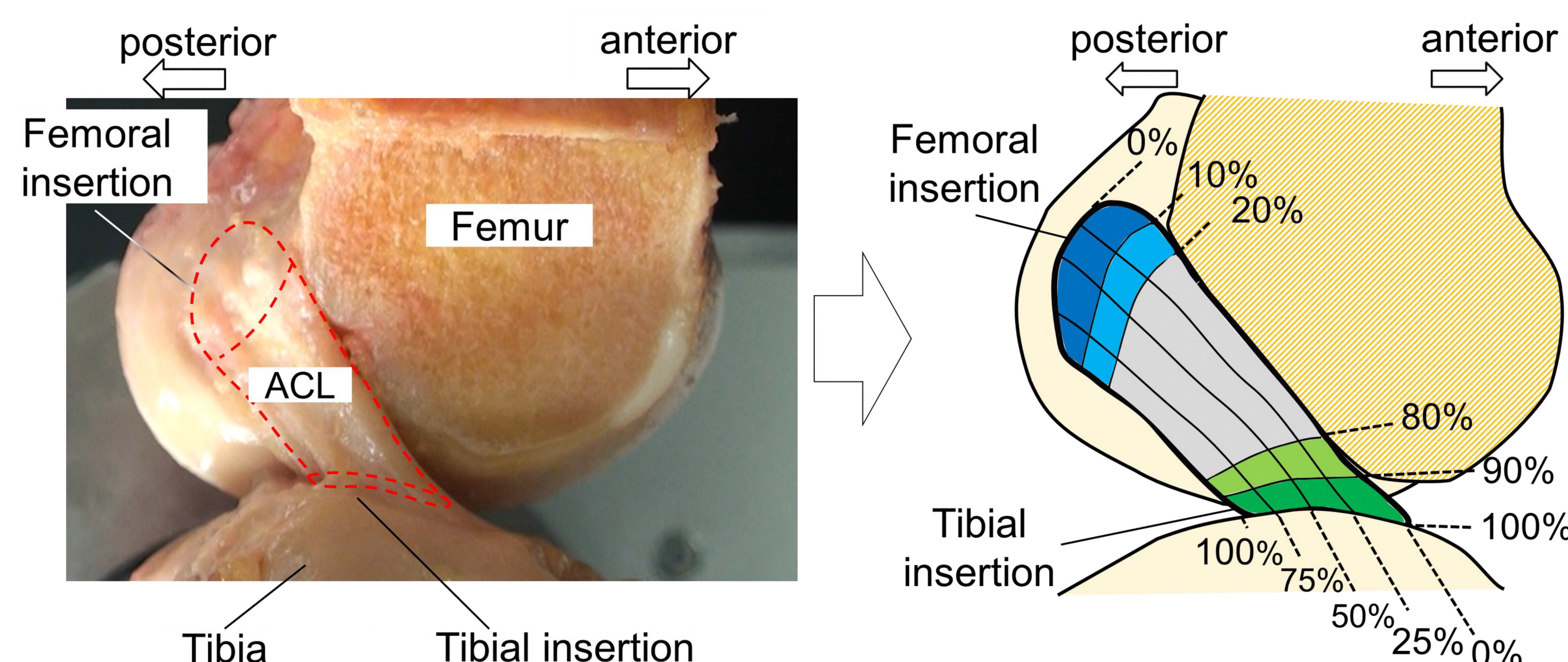


Figure 2: 20 portions on the ACL surface layer for the strain distribution (blue regions: femoral insertion area, green regions: tibial insertion area)

### Results

Strain distribution in both native and reconstructed ACLs in response to external knee loading was:

- Similar at full extension
- Different at 30 degrees of flexion especially in posterior fibers

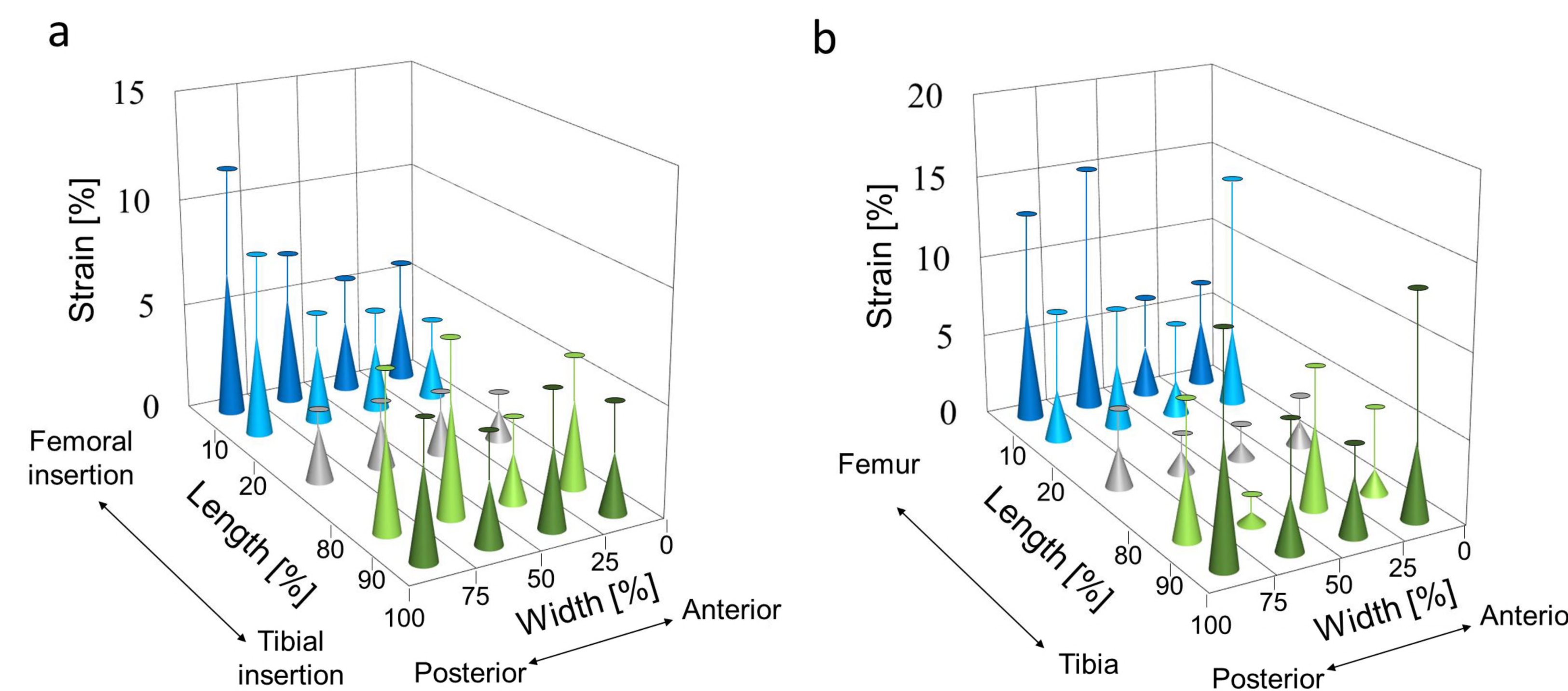


Figure 3 Strain distribution in native ACL (a) and reconstructed ACL (b) in response to 100 N of anterior tibial load at full extension (mean ± SD)

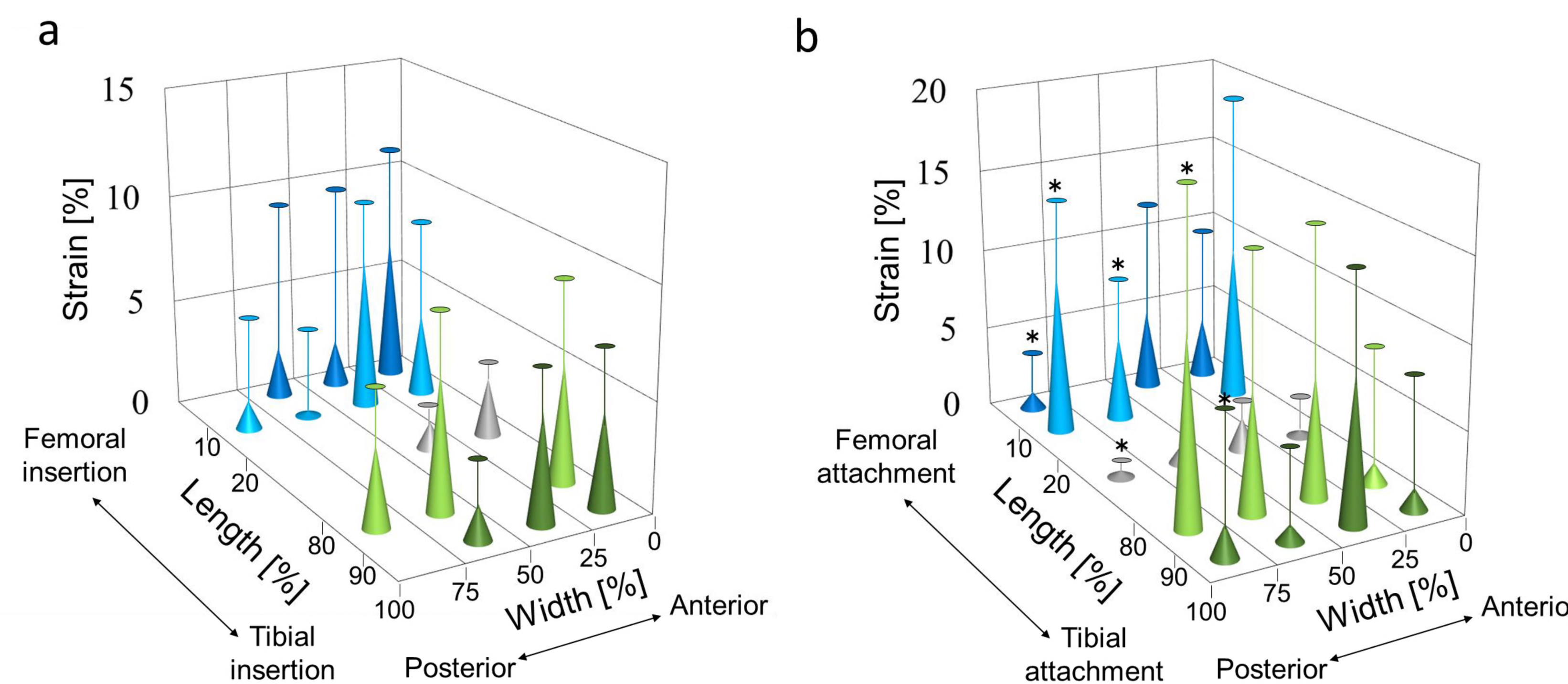


Figure 4 Strain distribution in native ACL (a) and reconstructed ACL (b) in response to 100 N of anterior tibial load at 30 degrees of flexion (mean ± SD, \* p < 0.05 vs native ACL)

### Conclusion

ACL reconstruction results in similar strain distribution at full extension but different strain distribution at 30 degrees of flexion, particularly in the posterior fibers.

### References

1. [1] [2] [3] [4] [5] [6] [7] [8] [9] [10] [11] [12] [13] [14] [15] [16] [17] [18] [19] [20] [21] [22] [23] [24] [25] [26] [27] [28] [29] [30] [31] [32] [33] [34] [35] [36] [37] [38] [39] [40] [41] [42] [43] [44] [45] [46] [47] [48] [49] [50] [51] [52] [53] [54] [55] [56] [57] [58] [59] [60] [61] [62] [63] [64] [65] [66] [67] [68] [69] [70] [71] [72] [73] [74] [75] [76] [77] [78] [79] [80] [81] [82] [83] [84] [85] [86] [87] [88] [89] [90] [91] [92] [93] [94] [95] [96] [97] [98] [99] [100]

### 5 W\_bck `YX[ Ya YbHg

ACL reconstruction results in similar strain distribution at full extension but different strain distribution at 30 degrees of flexion, particularly in the posterior fibers.

### F YZf YbWg

ACL reconstruction results in similar strain distribution at full extension but different strain distribution at 30 degrees of flexion, particularly in the posterior fibers.